Visibility, visual awareness, and visual masking of simple unattended targets are confined to areas in the occipital cortex beyond human V1/V2

Peter U. Tse1, Susana Martinez-Conde2, Alexander A. Schlegel1, and Stephen L. Macknik3,4

1Department of Psychological and Brain Sciences, Dartmouth College, H.B. 6207, Moore Hall, Hanover, NH 03755; and 2Barrow Neurological Institute, 350 West Thomas Road, Phoenix, AZ 85013

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In visual masking, visible targets are rendered invisible by modifying the context in which they are presented, but not by modifying the targets themselves. Here, we localize the neuronal correlates of visual awareness in the human brain by using visual masking illusions. We compare monoptic visual masking activation, which we find within all retinotopic visual areas, with dichoptic masking activation, which we find only in those retinotopic areas downstream of V2. Because monoptic and dichoptic masking are equivalent in magnitude perceptually, the present results establish a lower bound for maintenance of visual awareness of simple unattended targets. Moreover, we find that awareness-correlated circuits for simple targets are restricted to the occipital lobe. This finding provides evidence of an upper boundary in the visual hierarchy for visual awareness of simple unattended targets, thus constraining the location of circuits that maintain the visibility of simple targets to occipital areas beyond V1/V2.

Materials and Methods

Psychophysics. Subjects (n = 5) were given a brightness matching task while in the magnet. The three target conditions [Target-Only, SW1 (a visual masking illusion called “The Standing Wave of Invisibility”), and Control] were presented on the left half of the screen, whereas a luminance-adjustable Target-Only stimulus was presented on the right half of the screen. The bars along the vertical meridian were removed so that the left and right stimulus sets would not potentially mask each other. Each subject’s task was to adjust the luminance of the adjustable Target-Only side to match the appearance of the target in the left half of the screen. Stimuli were black (lowest possible luminance from the display system) on a white background (maximal luminance). To generate the Target Visibility Rating, subject luminance ratings were inverted and normalized to between 0 and 1, where 1 was the highest possible visibility of a black target on the display system and 0 was the lowest possible visibility.

fMRI. Seventeen healthy right-handed volunteers (of both genders between the ages of 18 and 40) were used for the monoptic study, and 14 of these returned for the dichoptic study, which was carried out on a different day. All had normal depth perception and normal or corrected-to-normal visual acuity. Subjects were paid $20 per session. Most subjects were scanned on 3 separate days, with one session each day: monoptic study, retinotopic mapping, and dichoptic study. To be clear: “monocular” means “with respect to one eye,” “monoptic” means “monocular” or “same in both eyes,” “binocular” means “with respect to both eyes,” and “dichoptic” means “different in the two eyes.” All of our stimuli were binocular, but, in monoptic conditions, both the target and mask were presented...
movements were removed by using the motion correction algorithm corrected to have the same mean intensity. Functional data were fact that slices were not collected at the same time. Slices were Tse et al. (40). We collected standard T2*-weighted echoplanar functional images using a head coil. Different biological tissues have different NMR relaxation time), T2 (spin-spin relaxation time), or T2* (relaxation time in the presence of local magnetic field inhomogeneities). These are known as T1-weighted, T2-weighted, and T2*-weighted images (40). We collected standard T2*-weighted echoplanar functional images using 25 slices [4.5-mm thickness and 3.75 × 3.75-mm in-plane voxel resolution, inter-slice distance 1 mm, repetition time (TR) = 2,500 ms, flip angle = 90°, field of view = 240 × 240 × 256 mm, interleaved slice acquisition, matrix size = 64 × 64] oriented approximately along the anterior-commissure posterior-commissure plane. These slices were sufficient to encompass the entire brain of each subject. Cushions were used to minimize head motion. A T1-weighted anatomical image with the same slice orientation as the echo-planar imaging (EPI) was collected for each subject, as was T2-weighted high-resolution anatomical scan.

Stimuli were projected onto a Plexiglas screen outside the bore of the magnet and viewed by means of a tangent mirror inside the magnet that permitted a maximum of 22° × 16° visible area. The projected image was smaller than this area and subtended ~17° × 12°. The experiment had a block design with 11 (5 condition and 6 fixation) 20-s blocks. Each run began with 10 s of dummy scans (four volumes that were discarded) to bring spins to baseline. Each run thus lasted a total of 230 s. Condition order was randomized on each run. Subjects carried out a minimum of 10 runs each and a maximum of 15. The first and last blocks were always fixation-only, and condition blocks were always separated by a fixation-only block. An entire cortical volume was scanned eight times per 20-s block (each block consisted of 40 cycles of the stimulus, duty cycle = 500 ms). Each 500-ms trial was cycled 40 times (20 s per block). In the monoptic sessions, each run of four blocks (presented in random order with interdigitated 20-s blank periods) lasted 3 min. In the dichoptic sessions, the total number of conditions was six (target and mask were each presented to the two eyes separately, doubling the conditions). Each run of six blocks (presented in random order with interdigitated 20-s blank periods) lasted 3 min after spins were brought to baseline.

We controlled for eye movements, wakefulness, and attention to the fovea by requiring subjects to perform a demanding reaction-time task in which the subject had to respond, within 500 ms (by means of button press), to a randomly occurring and slight change in fixation point color. The fixation point was 0.2° × 0.2° and changed color on average about once every 1.5 s. This color change took place an equal number of times during each block. No motor areas were found to be activated differentially between conditions, corroborating that the motor task was equivalent across all conditions. This task could be carried out successfully only if the subject was fixating during both condition and fixation-only blocks and attending to the fixation point carefully. Subject performance was 92.5% correct or better during each run or the run was not analyzed further. Thus, subjects were permitted an average of only one miss or delayed response per block.

Data were analyzed offline by using BRAIN VOYAGER (BV) 4.9.6 and MATLAB software developed in-house. Effects of small head movements were removed by using the motion correction algorithm in BV. Slice scan time correction was carried out to correct for the fact that slices were not collected at the same time. Slices were corrected to have the same mean intensity. Functional data were not smoothed in the space domain, but low-frequency temporal fluctuations were removed through high-pass filtering by convolving a one-dimensional Gaussian kernel with the time course on a voxel-by-voxel basis. This filter did not introduce correlations between a voxel and its neighbors.

Retinotopy was carried out by using standard phase-encoding techniques (21) (4.5-mm thickness and 3.75 × 3.75 mm in-plane voxel resolution, inter-slice distance 1 mm, TR = 1,600 ms, flip angle = 90°, field of view = 240 × 240 × 256 mm, interleaved slice acquisition, matrix size = 64 × 64; 16 slices oriented along the calcarine sulcus), with the modification that two wedges of an 8-Hz flicker black and white checkerboard grating were bilaterally opposite like a bowtie, to enhance signal to noise. Wedges occupied a given location for 2 TRs (3.2 s) before moving to the adjacent location in a clockwise fashion. Each wedge subtended 18° of 360°. An amount equal to 9.6 s (6 TRs of dummy scans) was discarded before each run to bring spins to baseline. On each run, 168 volumes were collected. A minimum of seven wedge runs was collected for each subject and then averaged to minimize noise before retinotopic data analysis in BV 4.9.6. A minimum of three runs was collected per subject by using expanding 8-Hz flickering concentric rings that each spanned ~1° of visual angle in ring width. Each ring was updated after one TR (1.6 s), after which it was replaced by its outward neighbor, except that the outermost ring was replaced by the innermost ring, whereupon the cycle was repeated.

Results

Psychophysical Analysis of Target Visibility. We presented a visual masking illusion called SWI (16, 22, 24, 25). The SWI is a combination of forward and backward masking in which the target and the mask about but do not overlap each other spatially or temporally. Fig. 1A describes the temporal sequence during a single monoptic SWI trial, as well as the sequences from the three other conditions tested. The SWI configuration used here optimized the retinal coverage of
both the target and mask stimuli to evoke the greatest possible BOLD signal. Monoptic fMRI sessions were also presented with a control condition (shown in Fig. 1A, for a total of four monoptic conditions) in which the timing of the standing wave was altered so that the targets were visible. Because the perceptual strength of monoptic masking is equivalent to that of dichoptic masking (16, 20), psychophysical testing of the new SWI configuration was conducted with monoptic stimuli only.

Fig. 1B shows the perceptual visibility of the target under the various target conditions. The results quantify the experience of the subjects: The targets in the Target-Only and Control conditions were highly visible although the target in the SWI condition was low in visibility (one-way ANOVA, \( F = 37.62, R^2 = 0.8625, P < 0.0001 \)).

**Upper Boundary for Masking of Simple Targets.** Fig. 2A shows significant functional activation to the Target-Only condition (blue and yellow voxels; \( P < 0.05 \) corrected, random effects analysis), after subtracting the voxels that responded significantly in the Mask-Only condition (\( P < 0.05 \) corrected, random effects analysis). This region of interest (ROI) defines the subset of cortical voxels that responded well to the target but not to the mask. Voxels that constitute circuits responsible for the visibility of targets presumably lie within this target-responsive ROI. These visibility-correlated voxels should moreover generate greater BOLD response to target-visible rather than to target-invisible conditions. We measured the responses of the two orthogonal conditions: Control (target-visible) and SWI (target-invisible) to determine the voxels that could potentially contain the neural correlates of target visibility (yellow, \( P < 0.01 \) uncorrected, random effects analysis). We found that these target visibility-correlated (yellow) voxels overlapped a subset of the target-responsive (blue) voxels. In this initial comparison, we used uncorrected statistics to liberally specify all possible regions that could potentially correlate with target visibility, including those regions that may show spurious correlations. Despite our use of liberal thresholds, only the occipital cortex produced activation. This result suggested that the circuits that maintain the awareness of target visibility may be confined to the occipital cortex. We ascertained the statistical significance of the occipital localization by comparing the average Control (target-visible) BOLD response with the average SWI (target-invisible) BOLD response in target-responsive ROI voxels within and outside the occipital cortex. The difference between Control and SWI conditions within occipital ROI voxels was averaged, and statistical significance was verified (Fig. 2B; Wilcoxon signed rank paired two-tailed \( t \) test, \( P = 0.0039 \) corrected, random effects analysis). We tested nonoccipital ROI voxels with the same analysis (Fig. 2C) and found no significant difference.

Although significant target responses were found in virtually all visual areas of the cortex (Fig. 2A, blue and yellow), we found visibility-related effects only in the occipital cortex (Fig. 2A, yellow). These results suggest that awareness of simple unattended targets, such as those used in the SWI, is generated by circuits within the occipital cortex.

One alternative interpretation of this result is that, whereas there may be visibility-related activity in the occipital lobe, the absence of visibility-related activity in nonoccipital areas may be due to regional cerebral blood flow differences, which would constitute a null-result. We addressed this possibility by comparing the occipital versus nonoccipital BOLD responses with the combined nonillusive conditions (Target-Only and Mask-Only). Occipital BOLD responses to nonillusory stimuli (Fig. 2D, purple) were weaker than nonoccipital BOLD responses (Fig. 2D, green; Wilcoxon signed rank paired two-tailed \( t \) test, \( P = 0.0001 \) corrected, random effects analysis). Therefore, rather than having misinterpreted a null-result, we have instead underestimated the significance of our occipital localization findings.

**Retinotopic Analysis.** To study the visual hierarchy within the occipital lobe further, we used retinotopic analysis of the occipital visual areas (21), and delineated the ROIs for areas V1, V2, V3, V4, V5, and V6 in each of the subjects tested. Fig. 3 shows the retinotopy results from two subjects.
Lower Boundary for Masking of Simple Targets. Within each retinotopic area (averaged across hemispheres), we determined the average BOLD response for the Target-Only, Mask-Only, and SWI conditions (monoptic and dichoptic presentations) across subjects. To determine the amount of masking present in each area, we calculated the percentage difference of the SWI BOLD response as a function of the Mask-Only BOLD response (Fig. 4A). If the difference was < 0, the target response was not suppressed during the SWI condition, but rather the target added to the overall BOLD response. If the increase was ≥ 0, the target response did not add to the mask response in the SWI condition: the target response was suppressed and therefore correlated with the perception of masking. The mask response may have been partially suppressed in the SWI condition as well [due to reciprocal masking by the target, as is commonly seen in primate physiology with this illusion (16, 24)].

All of the retinotopic occipital visual areas exhibited target visibility-correlated responses when the stimuli were presented monoptically (Fig. 4B). This result agrees with and follows from previous electrophysiological data from the awake primate, showing monoptic suppression of the masked target in the lateral geniculate nucleus (LGN) and area V1, presumably due to the action of lateral inhibitory networks (16, 24, 26). As in the previous primate results, dichoptic SWI masking responses in humans were not found in V1 (16) or in dorsal or ventral V2 (V2d and V2v), but only in subsequent retinotopic areas of the visual hierarchy (Fig. 4 B and C). Because dichoptic and monoptic visual masking are perceptually equivalent in magnitude (16, 20), the current data suggest that dichoptic BOLD responses could first correlate with the perception of simple targets in areas V3d, V3v, V3A/B, and V4v.

Further analysis of the strength of dichoptic visual masking in the dorsal and ventral visual streams suggests that dichoptic visual masking builds up over successive visual areas in the hierarchy (Fig. 4C; dorsal, $R^2 = 0.90$ and ventral, $R^2 = 0.72$). The dorsal stream exhibited a slightly higher %BOLD increase as a function of stage within the visual hierarchy ($F_{(1, 3)} = 17.16, P < 0.0001$). These
In the present study, we measured the BOLD activity underlying visual awareness during monoptic and dichoptic masking in humans. With masking, one can compare the perceptual and neural strengths of both monoptic and dichoptic target suppression. This comparison supplies a means to quantify the strength of target suppression and also to determine whether a weak suppression of the target may be due to the weakness of interocular suppression in the circuit tested, or to the lack of masking components within the circuit.

Implications for Lateral Inhibition Models of Visual Masking. Macknik and Martinez-Conde (16) previously recorded the responses of single neurons in the lateral geniculate nucleus (LGN) and primary visual cortex (V1) of awake monkeys to monoptic and dichoptic forms of the SWI illusion, and found that neither LGN nor V1 responses correlated with perception of dichoptic targets. To investigate the role of specific areas within the human occipital lobe in maintaining awareness, the present study mapped the retinotopic regions of the occipital lobe of each subject and then presented the SWI illusion monoptically and dichoptically to compare the responses in the retinotopic visual areas. Because monoptic and dichoptic visual masking are perceptually equivalent in magnitude (16, 20), only those areas with equivalent BOLD activity in monoptic and dichoptic masking conditions can potentially maintain visual awareness. Our results show that target suppression during monoptic masking is strong in all retinotopic occipital areas, but dichoptic masking builds up within the visual cortex and becomes strong only downstream of both dorsal and ventral V2 (i.e., within areas V3v, V3d, V3A/B, and V4v). These findings match previous primate single-unit recording results for area V1 (16), suggesting that area V1 plays a similar role in monkey and human visual awareness.

The ubiquitous strength of monoptic masking in the occipital retinotopic areas and the build-up of dichoptic masking strength in the extrastriate visual hierarchy are both predicted by the previous discovery that lateral inhibition builds up iteratively within the early visual system (16, 28). Unlike monoptic lateral inhibition, which begins in the retina and builds up to full strength in the striate cortex, lateral inhibition between the eyes (interocular suppression) begins to develop only in the binocular circuits of the striate cortex, and we show here that it does not reach full strength until the areas V3A/B and V4v (which may be hierarchically equivalent levels in the respective dorsal and ventral visual processing streams). We suggest that there are both lower and upper bounds within the visual hierarchy for the processing of visual masking and the maintenance of visual awareness of simple unattended targets; the lower bound is at least as high as the border between V2 and V3, and the upper bound is within the occipital lobe, possibly somewhere downstream of V4.

The dichoptic masking results are consistent with previous conclusions drawn from recordings in primates using binocular rivalry stimuli (27), in which perception-correlated processing was concluded to begin in the visual hierarchy as late as area V4. A later fMRI study conducted with motion-based rivalry in humans furthermore supports the idea that motion-based rivalry could not be maintained until human area V3A (17). Therefore, our current results, which suggest that visual awareness may be processed as
early as human V3 and V4, are consistent with previous primate results and some of the previous human results found with binocular rivalry stimuli.

Implications for Occipital vs. Nonoccipital Models of Visual Awareness. We found differing ratios of monoptic vs. dichoptic masking in occipital areas downstream of V2 (Fig. 3B), which may indicate that these areas do not maintain awareness of simple unattended targets, because dichoptic and monoptic masking are equivalent in strength psychophysically (16, 20). It is thus possible that the activation strength of monoptic versus dichoptic masking fully equilibrates only downstream of the retinotopic areas studied here, albeit somewhere within the occipital lobe. Nevertheless, the current data indicate that areas V1 and V2 fail to correlate with the perception of dichoptic masking, even though they contain circuits capable of processing visual masking (i.e., monoptically). These areas can therefore be ruled out as sufficient to maintain visual awareness, whether by themselves, or in concert with earlier subcortical areas. Our results thus suggest that visual masking of simple targets can be explained through occipital models, rather than with models of masking that require feedback or nonoccipital circuits (13, 25, 29, 30).

Care should be taken not to generalize these results to claims about the neural correlates of awareness of objects more complex than the simple targets used here. For instance, it is possible that complex visual stimuli such as faces and hands [known to be physiologically processed outside the occipital lobe (31, 32)] require activity in visual areas downstream of the occipital lobe to maintain awareness. Similarly, circuits that maintain the awareness of other types of visual processes, such as motion perception, may lie outside the occipital cortex (33). For example, Dehaene et al. (14) found neural correlates of word-priming masking outside of the occipital cortex. It is also possible that attended stimuli, including simple targets, may also invoke extraoccipital activation in a task-dependent manner (34).

Attentional Feedback and the Role of Area V1 in Human Visual Awareness. Haynes, Driver, and Rees (18, 19) have recently published two articles showing the BOLD correlates of monoptic masking in the cortex. Our study is in agreement with one of these studies, which concluded that human area V1 alone cannot maintain awareness of stimulus orientation (19). However, our results do not agree with the second study (18), which suggested that target visibility is derived by the coupling of area V1 BOLD activity with fusiform gyrus BOLD activity. The reason for this discrepancy may lie in a potential confound of this second study: the V1 activation found by Haynes et al. (18) may not indicate target visibility, but rather top-down attentional feedback. This possibility is suggested by their use of a behavioral task that demanded active attention to the target during scanning, which is known to cause increased BOLD activity in human V1 (35). Several other fMRI studies concluding that V1 maintains awareness may also be explained by uncontrolled top-down attentional feedback (11, 12, 36). Our task, on the contrary, demanded attention to the fixation point only, precluding effects of attention to the target. Lee et al. (12) found that peripheral binocularly rivalrous traveling waves could be tracked in V1 by using fMRI and concluded that V1 must thus contribute to the maintenance of awareness. However, they also found that, when the subject was attending to a different task at the fixation point, the BOLD signal from the traveling waves decreased. This finding suggests that the traveling wave BOLD signal seen by the authors was due to attentional feedback and is thus equivocal concerning a role for V1 in awareness.

Implications for Theories of Consciousness. The present results may lend support for some theories of consciousness that are modular in form and are sustainable with intermediate level processes (23, 37–39).

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